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(54) **MULTI-COMPONENT KNEE IMPLANT ASSEMBLY WITH MULTIPLE ARTICULATING AND TRAVELING SURFACES**

623/20.17, 20.19, 20.21, 20.2, 20.22, 20.23,  
623/21.13, 21.16, 23.4

See application file for complete search history.

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**A61F 2/30** (2006.01)

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USPC ..... **623/20.22**; 623/20.14; 623/20.21

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USPC ..... 606/88; 623/17.14, 19.12, 20.14, 20.15,

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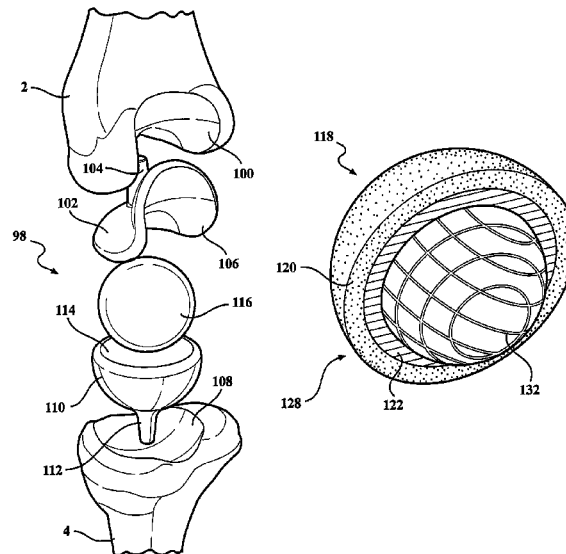
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(57) **ABSTRACT**

A multi-component joint assembly incorporated into reconditioned end surfaces established between an upper bone and an opposing lower bone. A first component is anchored into the upper reconditioned bone end surface and exhibits a first exposed support surface, a second component is anchored into the lower reconditioned bone end surface and exhibits a second exposed support surface. A spherical shaped and multi-directional supporting component is supported between the first and second anchored components.

**5 Claims, 8 Drawing Sheets**



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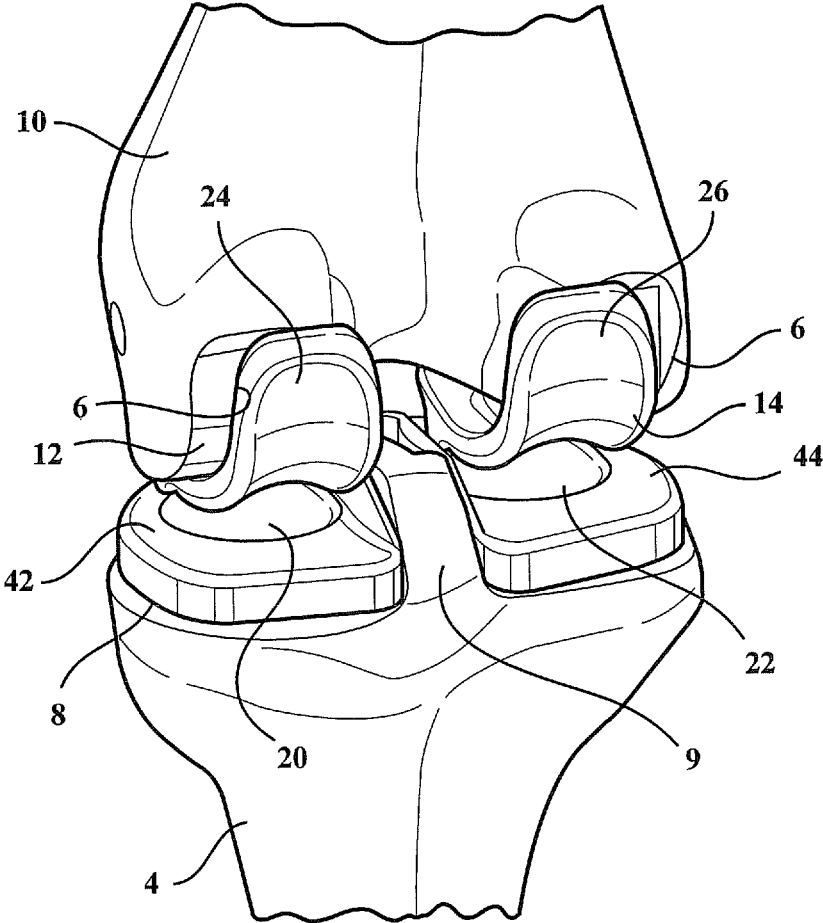


FIG. 1

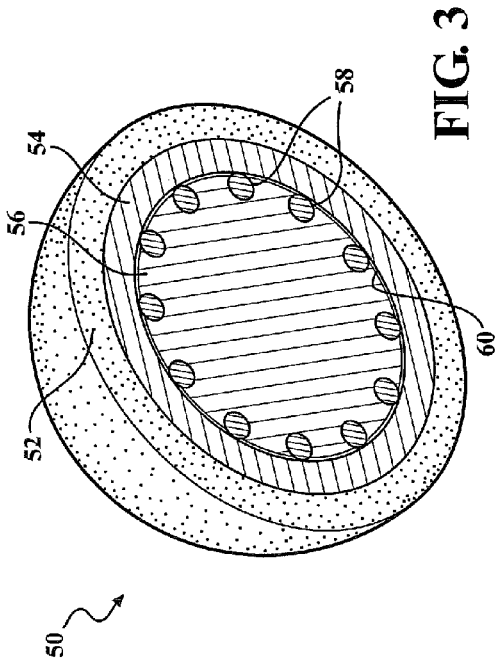


FIG. 3

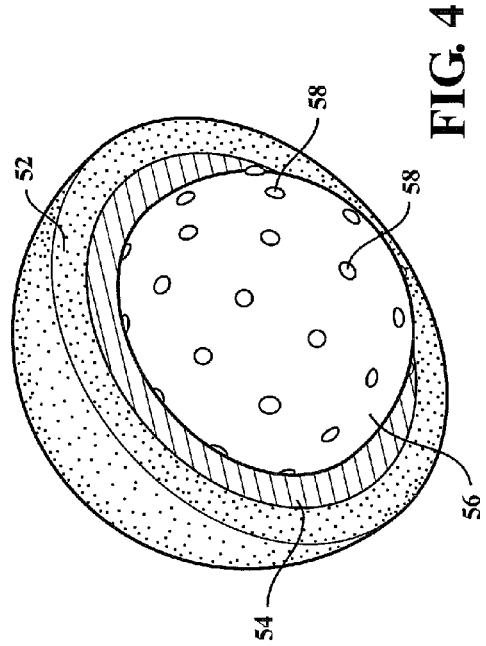


FIG. 4

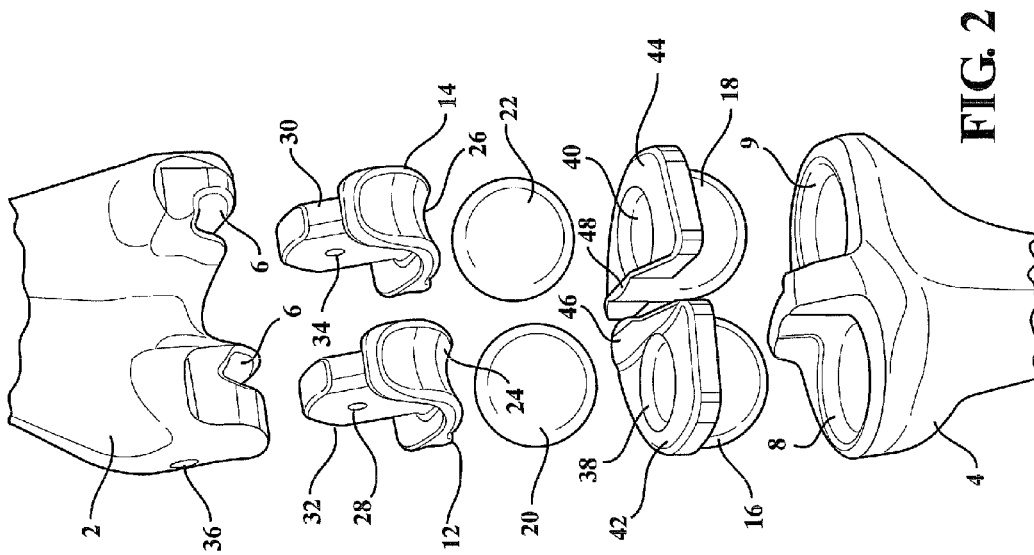


FIG. 2

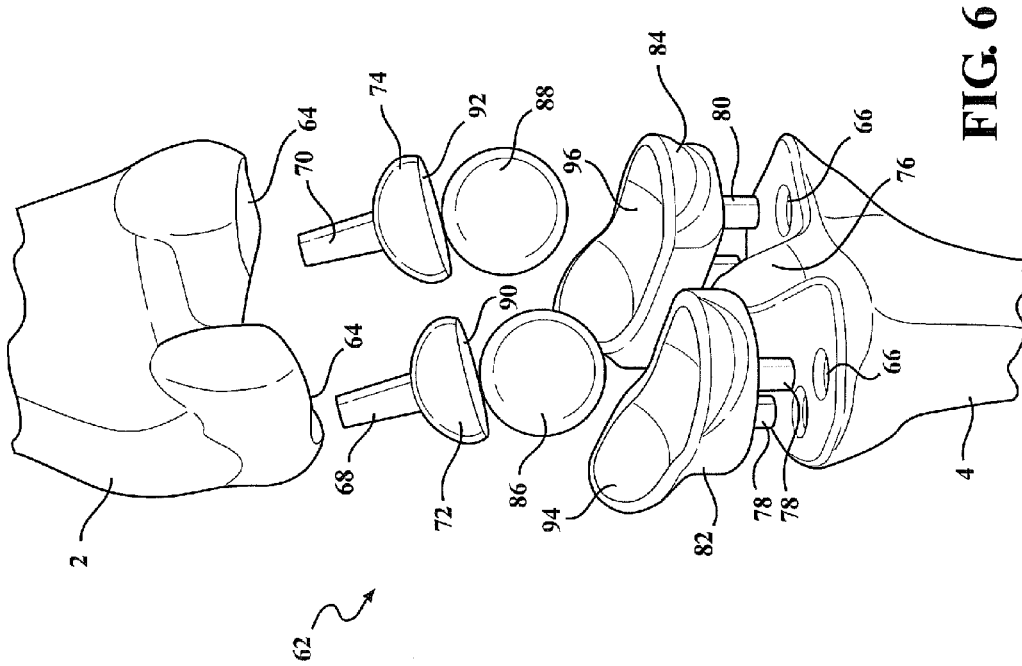


FIG. 6

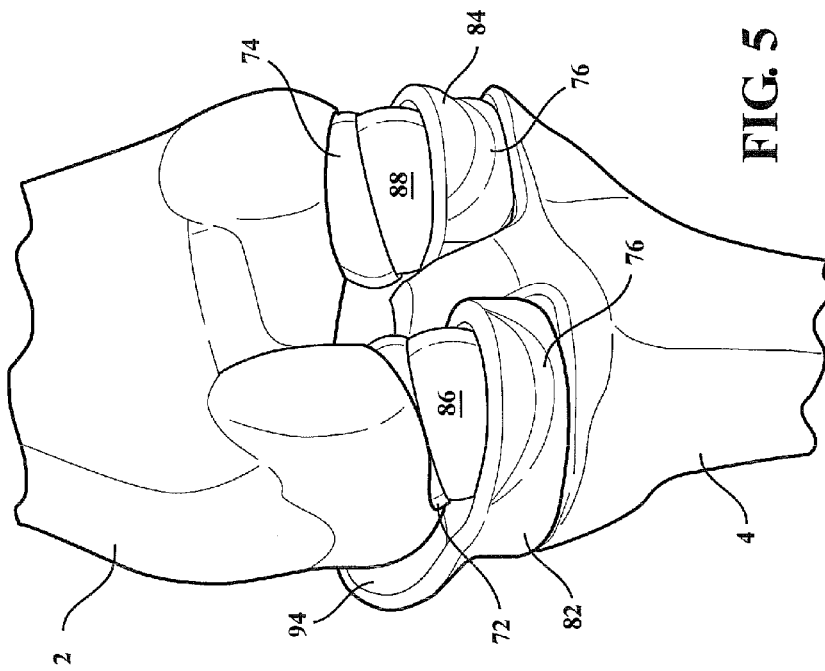


FIG. 5

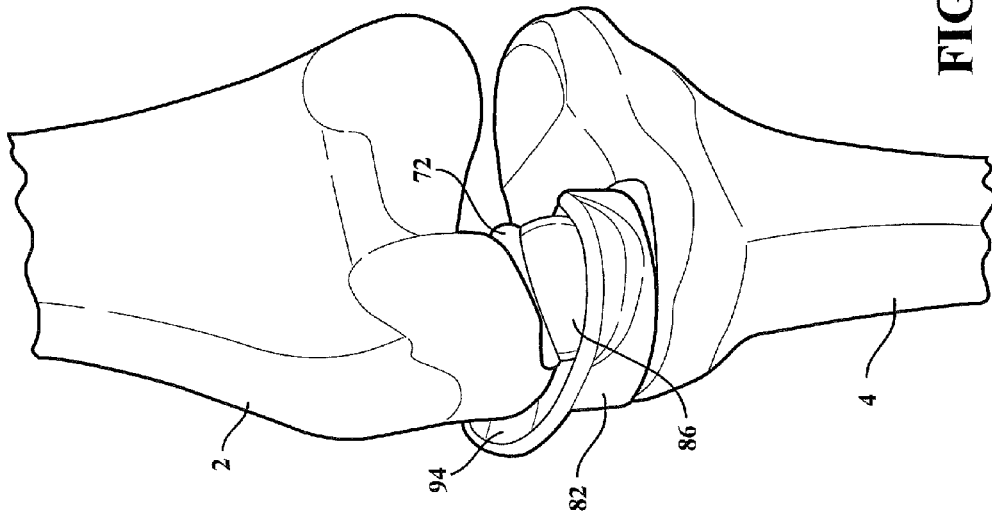


FIG. 8

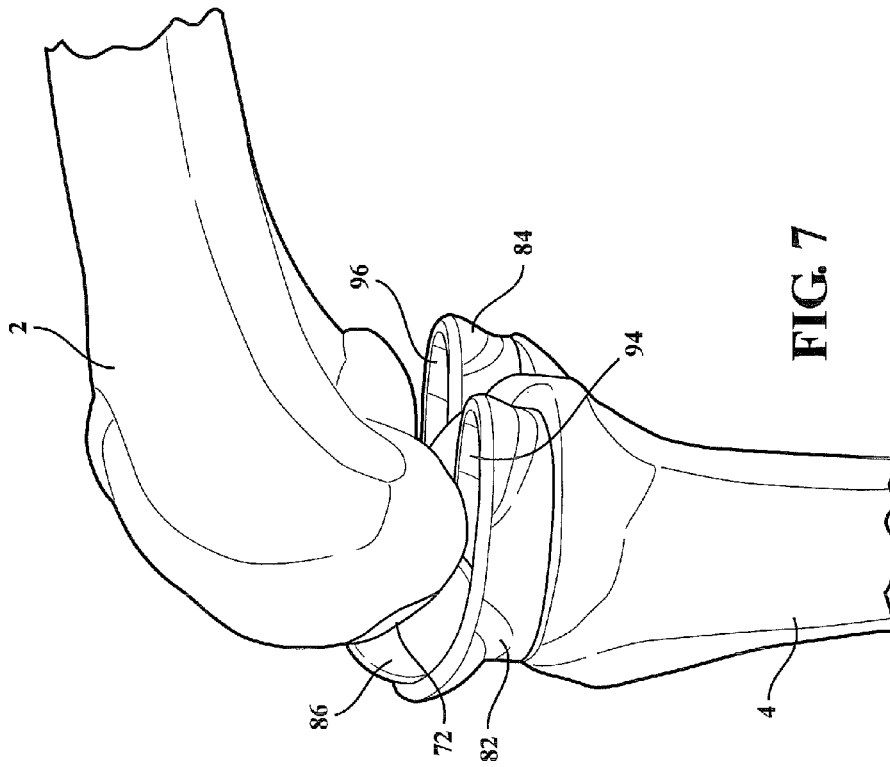


FIG. 7

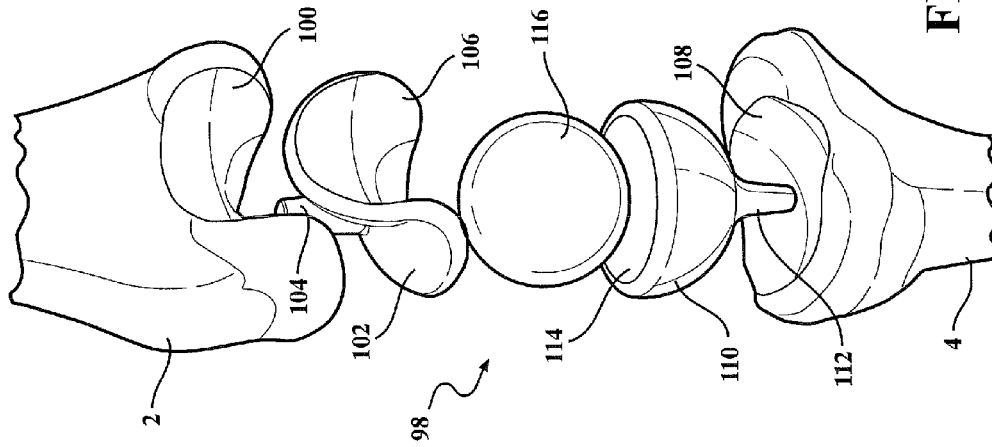


FIG. 10

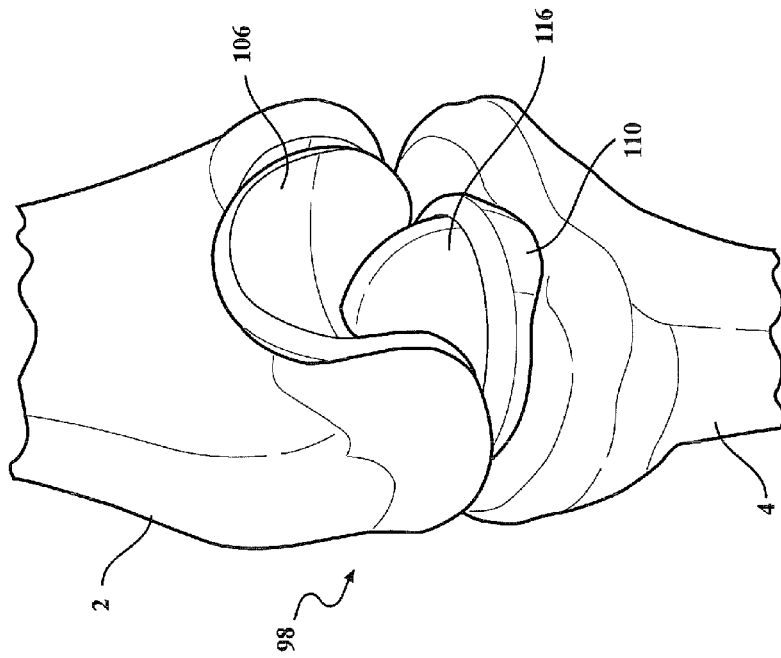


FIG. 9

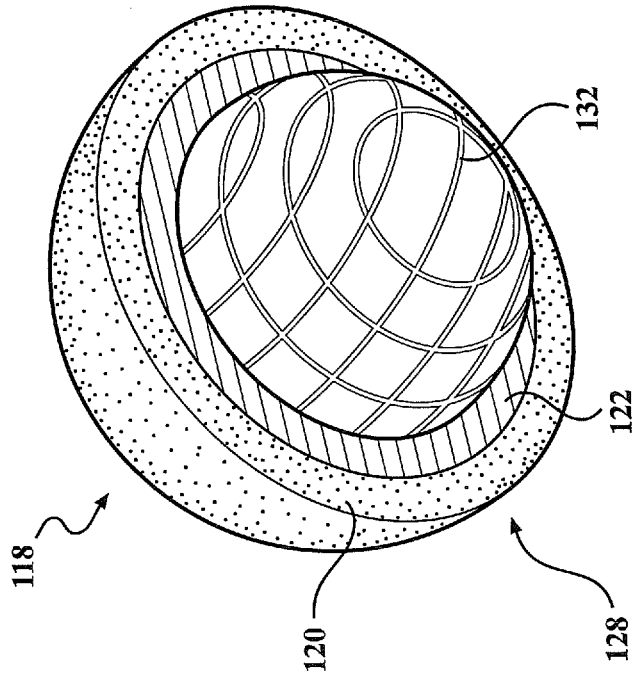


FIG. 12

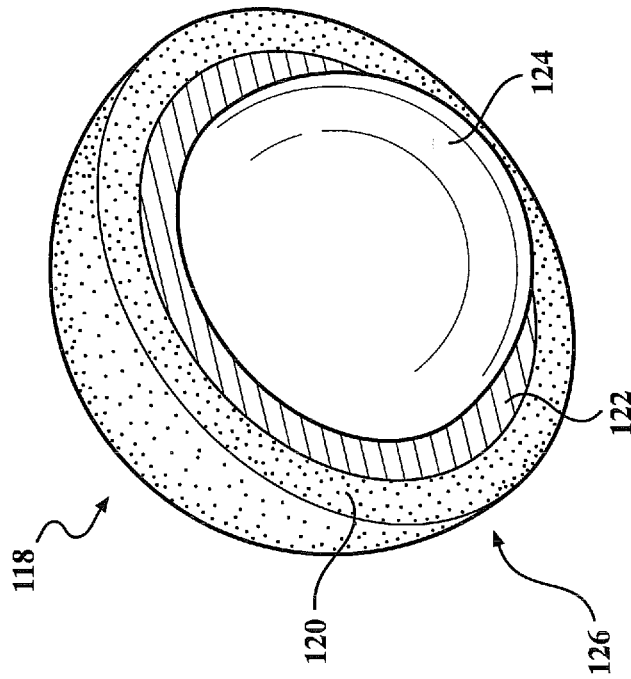


FIG. 11



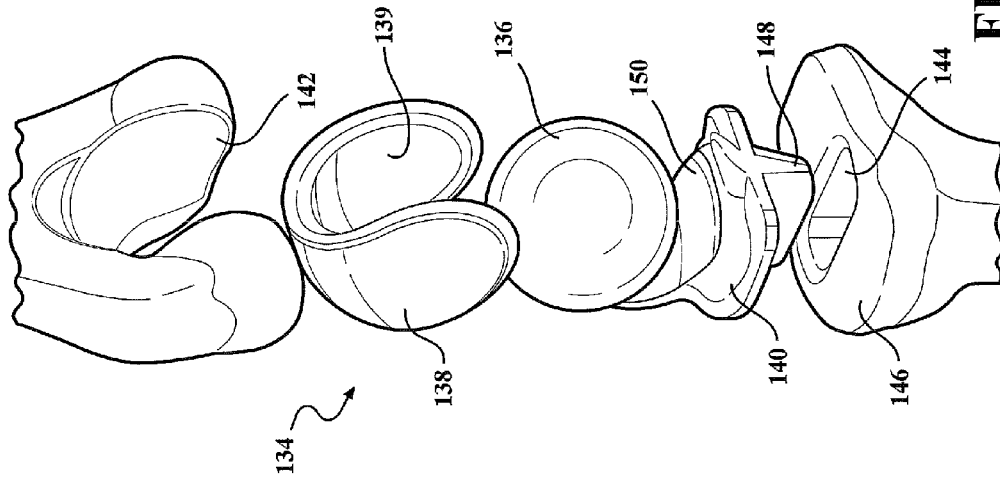


FIG. 14

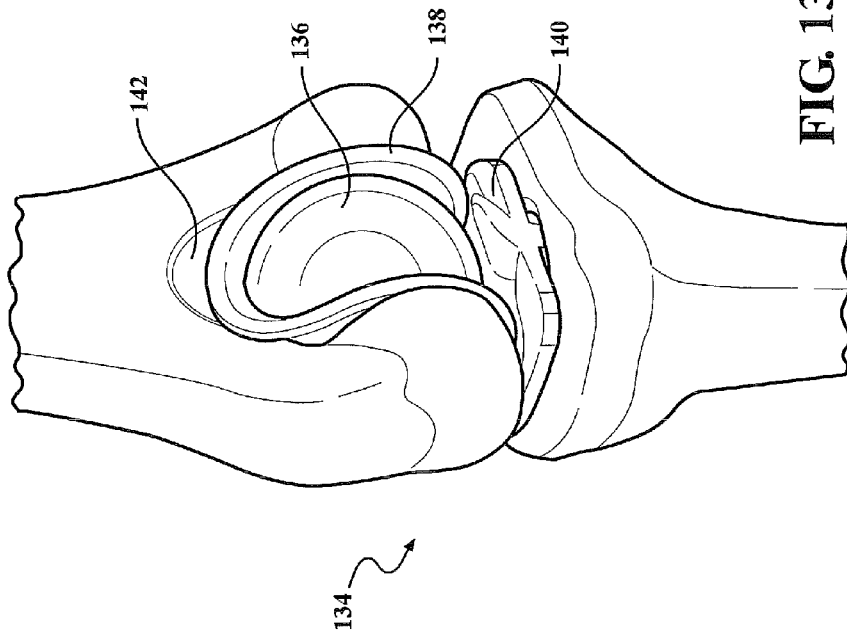


FIG. 13

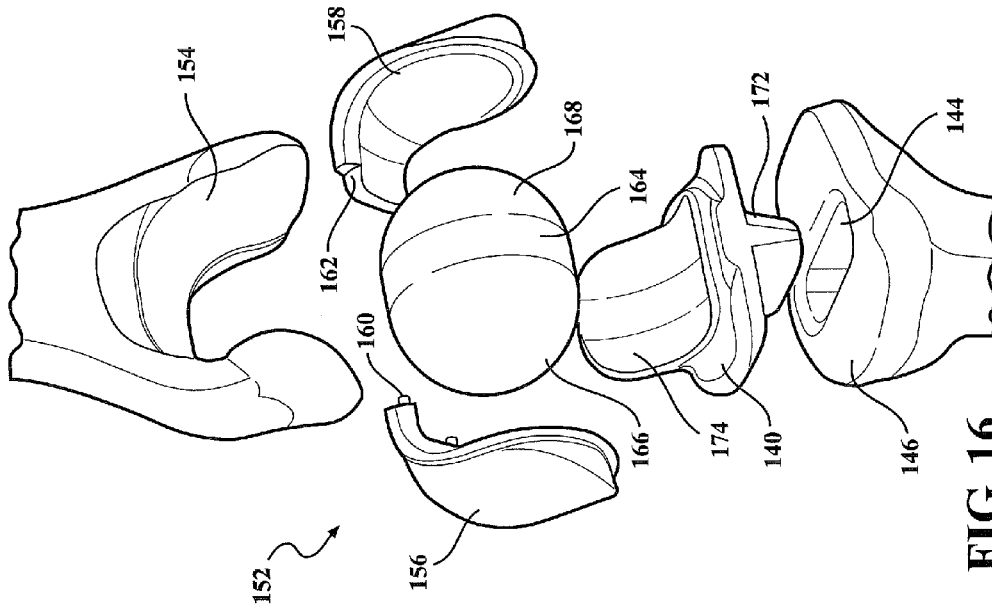


FIG. 16

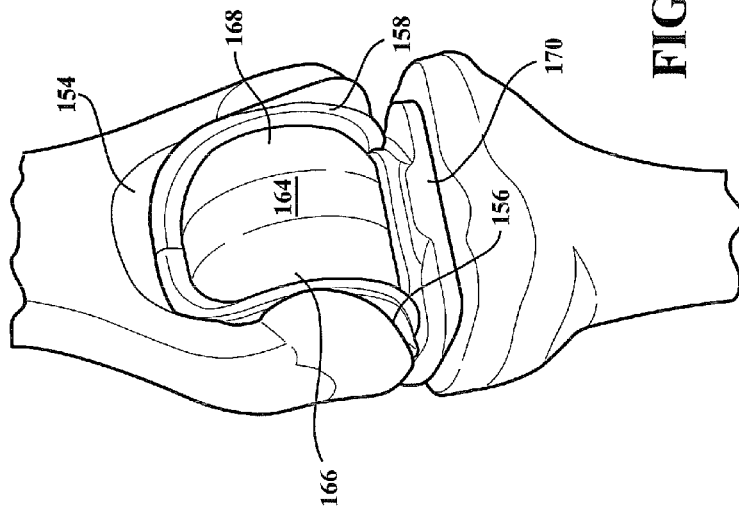


FIG. 15

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**MULTI-COMPONENT KNEE IMPLANT  
ASSEMBLY WITH MULTIPLE  
ARTICULATING AND TRAVELING  
SURFACES**

CROSS REFERENCE TO RELATED  
APPLICATIONS

The present application claims the priority of U.S. Ser. No. 61/526,708 filed Aug. 24, 2011.

BACKGROUND OF THE INVENTION

1. Field of the Invention

The present invention discloses an artificial joint assembly, such as is particularly configured for employing as a retrofit knee joint, and which combines multiple artificial components incorporated into first and second reconditioned joint defining surfaces for providing increased wear life in tandem with evenly distributed wear pattern/profile as well as enhanced flexibility and mobility.

2. Background of the Relevant Art

The prior art is well documented with examples of artificial knee implant assemblies. These include such as the spherical knee joint prosthesis of Bosredon, U.S. Pat. No. 6,117,175, the total knee implant of Byrd et al., US 2010/0191342 and the artificial implant component and method for securing disclosed in Elias, U.S. Pat. No. 5,480,443.

SUMMARY OF THE PRESENT INVENTION

The present invention discloses a multi-component joint assembly incorporated into reconditioned end surfaces established between an upper bone and an opposing lower bone. The assembly includes a first component anchored into the upper reconditioned bone end surface and exhibiting a first exposed support surface and second component anchored into the lower reconditioned bone end surface and exhibiting a second exposed support surface. A spherical shaped component is supported in at least one of eccentric rotational and linear/arcuate translatable fashion between the first and second anchored components.

Additional features include at least one of said components further exhibiting an arcuate and optionally inwardly flared track support surface. At least one of the components further exhibits a hemispherical recess for substantially seating the spherical shaped component. Other features of the joint assembly include each of the first, second and spherical shaped components further being constructed of at least one of a metal, plastic, polymer or composite material.

In other applications, a first pair of components are arranged at a first side of the assembly, with a second identical pair arranged at an opposite second side, such as is typical of a retrofit knee joint assembly. In this fashion, a subset pair of these components may further be employed in a 1/2 implant assembly associated with a selected side of the joint defining bones.

Other features include the spherical shaped component further exhibiting a multi-layer composition including a softer outer layer and at least one harder interior layer which can further include first and second inner layers establishing an eccentric rotational interface therebetween.

A plurality of surface projecting bearings are mounted within an innermost spherical shaped portion of the spherical component, these facilitating the eccentric rotational interface. A grid pattern of lubricating grooves defined in a surface

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of an innermost spherical shaped portion of said spherical component facilitating the eccentric rotational interface.

BRIEF DESCRIPTION OF THE DRAWINGS

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Reference will now be made to the attached drawings, when read in combination with the following detailed description, wherein like reference numerals refer to like parts throughout the several views, and in which:

10 FIG. 1 is a perspective view of a knee implant assembly according to a first embodiment of the invention;

FIG. 2 is an exploded view of the multi-component assembly of FIG. 1 and better illustrating the reconditioned end-configurations established between the upper femur and 15 lower tibia leg bones combined with the pairs of upper bone secured arcuate tracks, lower bone secured receiving troughs and intermediate positioned spherical inter-movable supports;

FIG. 3 is a cutaway view of a selected spherical inter-movable support and which illustrates its multi-material construction with softer outermost material, an intermediate 20 harder material, and an innermost harder materials, an eccentric rotatable interface established between said intermediate and innermost layers further incorporating encapsulated ball bearings;

FIG. 4 is an illustration similar to FIG. 3 and depicting the outermost and intermediate layers of the spherical support again in cutaway fashion, along with the innermost portion exhibited in three dimension perspective with surface supported bearings;

FIG. 5 is an illustration similar to FIG. 1 of a knee implant assembly according to a further preferred variant;

FIG. 6 is an exploded view of the multi-component assembly of FIG. 5 and better illustrating the reconditioned end-configurations established between the upper femur and 35 lower tibia leg bones combined with the pairs of upper bone secured concave seating supports, lower bone secured concave track profiles, and intermediate positioned spherical inter-movable supports;

FIG. 7 is an assembled and substantially side rotated perspective similar to FIG. 5 and depicting a substantially 90° bend established between the upper femur and lower tibia with associated combined eccentric rotation and forward lineal displacement of the intermediate spherical supports 40 within the lower bone affixed concave track profiles;

FIG. 8 is an illustration substantially identical to that previously depicted in FIG. 5 and presenting only a selected side or 1/2 implant assembly according to a further potential sub-variant;

FIG. 9 is an assembled view of a further knee implant assembly and exhibiting a single eccentric and inter-movable interface;

FIG. 10 is an exploded view of the implant assembly of FIG. 9 and better illustrating the reconditioned end-configurations established between the upper femur and lower tibia leg bones including an upper bone secured and inwardly 55 concave flared and pseudo arcuate shaped seating support, a lower bone secured concave support, and an intermediate positioned spherical inter-movable support and which, similar to the previous variants, is eccentrically rotatable at both upper and lower seating locations, combined with linearly/arcuately translatable such as in relation to the upper seating support;

FIG. 11 is an illustration of a spherical support associated with such as the variant of FIGS. 9 and 10 and presented 65 similarly to that previously depicted in FIG. 4 with a smooth faced and hard innermost portion exhibited in three dimen-

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sion perspective and in eccentric rotatable fashion relative to an intermediate harder material in turn encased within a softest outermost material;

FIG. 12 is an illustration largely identical to FIG. 11 of an alternately configured spherical support with lubricating grooves illustrated along an exterior spherical profile of the innermost hardened material;

FIG. 13 is an assembled view of a still further knee implant assembly analogous to that depicted in FIG. 9 and depicting an alternately configured single eccentric and inter-movable interface;

FIG. 14 is an exploded view of the implant assembly of FIG. 13 and better illustrating the reconditioned end-configurations established between the upper femur and lower tibia leg bones including an upper bone recess secured pocket, a lower bone secured arcuate/concave support, and an intermediate positioned spherical inter-movable support and which, similar to the previous variants, establishes a limited eccentrically rotatable configuration with the upper leg receiving pocket, combined with a further measure of eccentric support with the lower leg secured arcuate/concave support and again combined with a limited degree of linearly/arcuately translatable motion along the lower leg secured arcuate support pathway;

FIG. 15 is a perspective assembled illustration similar to that depicted in FIG. 14 and in which the upper bone recess secured pocket component and intermediate support are both reconfigured to accommodate a substantially intermediate flattened and pseudo roller/egg shaped support according to a yet further preferred variant; and

FIG. 16 is an exploded view of the implant assembly of FIG. 15 and better illustrating the reconditioned end-configurations established between the upper femur and lower tibia leg bones including first and second assembled and recess mounted components defining the upper bone recess secured pocket, a lower bone secured arcuate/concave support, and an intermediate positioned inter-movable support exhibiting the pseudo spherical/cylindrical flattened and elongated profile for establishing a more robust upper rotational support combined with like lower rotational support and limited arcuate/linear displacement.

#### DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

As will be disclosed with succeeding reference to the several depicted embodiments, the present invention discloses an artificial joint assembly, such as is particularly configured for employing as a retrofit knee joint, and which combines multiple artificial components incorporated into first and second reconditioned joint defining surfaces for providing increased wear life in tandem with evenly distributed wear pattern/profile as well as enhanced flexibility and mobility.

The joint assemblies described herein are particularly configured for such as in situ reconditioned installation within a patient's knee assembly (between the lower end of the upper femur bone and corresponding upper end of the lower tibia bone), however it is further understood that certain applications could in theory include other joint applications, either human or other mammalian. For purposes of ease and clarity of illustration, the various embodiments depicted further do not include reference to additional necessary components of the knee joints, such as including the patella (knee cap) and associated muscles, tendons and ligaments, the inclusion of which are assumed and which collectively define a functioning knee joint.

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Referring now to FIG. 1, a perspective view is generally shown at 10 of a knee implant assembly according to a first embodiment of the invention and which is incorporated between an upper leg (femur) bone 2 and a lower leg (tibia) bone 4 (and with which an associated fibula bone is also not depicted). The present invention contemplates such as in situ reconditioning of the bone ends, illustrated by conditioned end profiles 6 configured into the bottom most end surface of the femur 2, as well as opposing upper end facing and recessed profiles 8 defined in the upper most end of tibia 4 with additional bridging location 9 defined between the substantially hemispherical shaped recessed profiles 8. Such reconditioning occurs following incision or removal of any remaining damaged bone and/or cartilage associated with the damaged joint and during an appropriate surgical procedure utilizing medical drilling, boring and shaping instruments in order to recondition the joint defining bone ends and to create the desired shaping and profile of the joint. As previously indicated, it is advantageous to refashion the joint end profiles in situ during an appropriate surgical procedure, a further objective being to retain or repair, where possible, natural ligament, cartilage and muscle associated with a normal functioning joint.

Although not shown, such reconditioning can be employed with minimal interference to such necessary additional elements of the joint including each of the patella or knee cap, ligaments, muscles and tendons. Without limitation, it is further understood that the joint assemblies described in each of the illustrated variants can be integrated into either of human or synthetic bones (such as which can also contemplate both human and synthetic bones in a single joint application), with such joint assemblies also capable of surgically implanted in either total or partial (as depicted in FIG. 8) manner concurrent with any necessary degree of refashioning or removal of damaged bone or joint.

Referring to FIG. 1 again in collaboration with exploded view of FIG. 2, the multi-component assembly 10 better illustrates the reconditioned end-configurations 6 and 8 established between the upper femur 2 and lower tibia 4 leg bones combined with pairs of upper bone secured arcuate tracks 12 and 14, lower bone secured receiving troughs 16 and 18 (see as best shown in FIG. 2) and intermediate positioned spherical inter-movable supports 20 and 22. For purposes of the present description, a pair of implant components can also refer to a subset of upper and lower bone engaging implants as depicted in side-by-side fashion in FIG. 1 as well as 1/2 retrofit installed fashion as depicted in FIG. 8.

Each of the components a12-22 are constructed of any arrangement of metal, polymer, plastic, composite or other suitable material, with it further being understood that the individual pairs of components can be arrayed with any pattern of alternating materials, such that the outer (upper and lower affixed) pairs of components 12 & 14 and 16 & 18 can be constructed of a first material, with the intermediate positioned spherical (bearing) supports 20 and 22 being of a second material. In this fashion, the desired wear properties and profiles are adjusted in part based upon the material selection of the individual components with concurrent objectives being both equalization of overall wear patterns established between the respective pairs of components and determining those situations in which metal on metal or plastic on plastic contact between the components is either desired or, more often, not.

Both the upper bone secured tracks 12 and 14 and lower bone secured troughs 16 and 18 are anchored in seating fashion within the inner recessed profiles 6 and 8 of the femur 2 and tibia 4 bones by use of a suitable medical cement (it

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further being understood that suitable bone adhesion can also be assisted or promoted by inner marrow in given circumstances). The upper tracks **12** and **14** each exhibit and arcuate, inwardly flared exposed surface (see at **24** and **26** in FIG. **2**), with inner (reverse side) extending stems **28** and **30** recess mounting within mating recess configurations defined in the joint end defining face of the upper femur bone **2**. Width extending apertures **32** and **34** defined in the stems **28** and **30** can also receive widthwise inserting pins **35** (again FIG. **2**) extending through mating and aligning apertures formed widthwise through the femur bone **2** (see further at **36**).

The lower bone secured inserts exhibiting seating troughs **16** and **18** each further include a generally semi-spherical shaped body with bottom convex surfaces which seat within the mating three dimensional recess profiles **8** established within the joint end face defining profiles of the lower tibia **4**. The lower troughs **16** and **18** in turn exhibit upwardly facing and substantially semi-spherical inner recess **38** and **40** surrounded by upper lip or rim annular supporting edges **42** and **44**. Inner opposing edge profiles of the troughs **16** and **18** are further defined by upward raised projections exhibiting inner opposing edges **46** and **48** which seat against the raised bridge location **9** defined in a mid location of the tibia end face again in the manner depicted in the assembled view of FIG. **1**.

The spherical shaped supports **20** and **22** are dimensioned so that they substantially seat within the inner recesses **38** and **40** (see again FIG. **1**) upon being fully installed in the manner depicted in FIG. **1**. In this fashion, the spherical supports **20** and **22** establish rotatable eccentric support within the lower troughs **16** and **18** (in additional to a determined minor degree of side-to-side and/or fore-to-aft translation of the supports **20** and **22** within the troughs, such as due to designed tolerances within the recessed semi-spherical profiles **8**) combined with the inwardly flared and arcuate surfaces **24** and **26** of the upper arcuate tracks **12** and **14** (these being again exposed following anchoring of the tracks within the femur end surface) establishing like rotational support against upper corresponding edges of the spherical supports **20** and **22** combined with longitudinal/arcuate (fore and aft) support. In this fashion, the joint assembly distributes motion along two interfaces (between upper bone anchored tracks **12** and **14** and intermediate spherical bearing supports **20** and **22**, as well as separately between the bearing supports **20** and **22** and the lower tibia anchored troughs **16** and **18**).

This arrangement further enables the upper interface between the tracks **12** and **14** and spherical bearings **20** and **22** to permit the bearings to translate along the arcuate paths **24** and **26** defined in the upper tracks **12** and **14**, concurrent with its rotation at both the upper tracks and lower trough **16** and **18** interfaces, such as occurring during bending motion of the knee. As again previously indicated, additional configurations of muscles, ligaments, tendons and patella (knee cap) are provided and can include both natural (pre-existing) and/or synthetic materials, such as which are concurrently implanted or reconstructed in order to provide a dynamic and long-term implantable assembly.

Referring now to FIG. **3**, a cutaway view is generally shown at **50** of a selected spherical inter-movable support, such as again represented by each of **20** and **22** in FIGS. **1** and **2**. The cutaway view of FIG. **3** illustrates one non-limiting example of a multi-layer material construction and which includes a softer (typically plastic or plastic composite) outermost material layer **52**, an intermediate harder **54** material (typically another plastic), and an innermost harder material **56** (which can be of a similar hardness as the intermediate layer **54** as well as relatively harder or softer based on the preferences of the application).

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An eccentric rotatable interface is established between the intermediate **54** and innermost **56** layers, and which further includes a plurality of ball bearings **58** encapsulated within the inner most layer **56** with arcuate edge portions thereof projecting from the spherical surface thereof (see further in FIG. **4** which depicts the same variant with the exception that the innermost material **56** is depicted in three dimension relative to the outer planar cutaway layers). In this fashion, an inner encapsulated and rotational interface **60** established between an inner-most spherical body defined by the innermost layer **56** and its edge projecting and individually eccentric mounted bearings **58** and the opposing inwardly facing boundary of the intermediate layer **54** provides an additional measure of dynamic compress and multi-axial eccentric motion to complement the performance of such as the non-limiting joint application of FIGS. **1** and **2**.

Proceeding to FIGS. **5-7** in succession, an illustration similar to FIG. **1** is generally depicted at **62** of a knee implant assembly according to a further preferred variant and in which a different set of reconditioned and recess configured profiles within the joint defining end faces of the femur **2** and tibia **4** are defined respectively at **64** and **66** in the exploded view of FIG. **6**, respectively and in comparison to the configuration of the corresponding profiles **6** and **8** in FIG. **2**. As best depicted in the exploded view of FIG. **6**, the upper profiles **64** define reconfigured recesses for receiving inserting posts **68** and **70** associated with upper bone secured concave seating supports **72** and **74**, with the lower profiles **66** exhibiting spaced apart pairs of recessed mounting holes separated by a conditioned intermediate projecting bridge **76** (compare to at **9** in FIG. **2**) and receiving opposing and underside projecting mounting posts **78** and **80** forming portions of lower bone secured concave track profiles **82** and **84**.

A pair of intermediate positioned spherical inter-movable supports **86** and **88** are provided similar in nature to the corresponding supports **20** and **22** illustrated in FIGS. **1** and **2**, and which seat within concave recessed profiles **90** and **92** (see again as best shown in FIG. **6**) associated with the upper seating supports **72** and **74** as well as being supported upon inner flared and arcuate extending and upper facing track surfaces **94** and **96** associated with the lower track profiles **82** and **84**. FIG. **7** further depicts an assembled and substantially side rotated perspective similar to FIG. **5** and in which a substantially 90° bended position is established between the upper femur **2** and lower tibia **4**, with associated combined eccentric rotation and forward lineal displacement of the intermediate spherical supports **86** and **88** better illustrated within the lower bone affixed concave track profiles **94** and **96**, such occurring during maintenance of current ligament (meniscus) structure in most applications.

FIG. **8** is largely identical to FIG. **5** and presents only a selected side or 1/2 implant assembly according to a further potential sub-variant. The significance of FIG. **8** is to illustrate that sub-variants of the joint assembly can be incorporated into reduced or partial reconstructed applications, where applicable, and in situations where an entire reconstructed assembly is either unwarranted or unnecessary. Although not shown, the unreconstructed half of the joint assembly retains its original joint defining structure which, to the extent possible, is unaffected by the reconditioning performed to the implanted half of the joint assembly.

Proceeding on to FIGS. **9** and **10**, assembled and exploded views are generally shown at **98** of a further knee implant assembly and exhibiting a single eccentric and inter-movable interface. Specifically, and as best depicted in FIG. **10**, a reconditioned end-configuration **100** established within the upper femur **2** receives (such as again in a cemented or other

permanently affixing fashion) an inwardly concave flared and pseudo arcuate shaped seating support **102** (as best shown in FIG. **10**) which further exhibits a reverse face/inwardly projecting support post **104** anchoring into an aligning recess machined into the upper femur **2** (not shown), combined with the arcuate end surface profile **100** of the bone **2** mirroring the undulating pattern of the reverse/back surface of the arcuate support **102**. A corresponding outer facing surface **106** of the upper support **102** exhibits an inwardly flared and slightly elongated profile not dissimilar to a reverse saddle (or potato chip) shape.

A lower reconditioned surface profile, see at **108**, is configured within the joint defining end face of the tibia bone **4** and anchors a lower bone secured concave support **110** further exhibiting a lower extending mounting stem or post **112** received within a corresponding mating recess (not shown) associated with an innermost machined location of the lower profile **108**. The lower concave support **110** further exhibits an outwardly facing and substantially hemi-spherical bowl shape **114**.

A single and intermediate positioned spherical inter-movable support **116** and which, similar to the previous variants, is eccentrically rotatable at both upper and lower seating locations, combined with linearly/arcuately translatable such as in relation to the inner elongated surface **106** of the upper seating support **102**, while exhibiting both eccentric rotation as well as a limited degree of lateral or fore to aft adjustability within the seating pocket defined by the hemi-spherical bowl shape **114** within the lower anchored support **110**. It is further envisioned that the respective materials of the upper **102** and lower **110** supports can exhibit either the same or different properties which render them respectively harder or softer and this, combined with the material properties of the intermediate positioned spherical support **116** again assists in establishing varying dynamic operating properties.

FIG. **11** is an illustration in cutaway, generally at **118**, of a single spherical support associated with such as the variant of FIGS. **9** and **10**, and presented similarly to that previously depicted in FIG. **4**. The single support **118** includes a softest (cushioning) outermost layer **120**, a harder intermediate layer **122** and a smooth faced and similarly hard innermost spherical body defined by an outer surface **124** and which, similar to FIG. **4**, is exhibited in three dimension perspective and in eccentric rotatable fashion about an interface **126** established relative to the inner surface of the intermediate harder material layer **122**. FIG. **12** is an illustration largely identical to FIG. **11** of an alternately configured spherical support, see at **128**, and exhibiting a network of lubricating grooves **130** illustrated along an exterior spherical profile of an innermost hardened material **132**, with corresponding outermost softest **120** and intermediate harder **122** material layers again provided as previously described.

FIGS. **13** and **14** depict, generally at **134**, assembled and exploded views of a still further knee implant assembly analogous to that depicted in FIG. **9** and depicting an alternately configured single eccentric and inter-movable interface defined between a single spherical and intermediate component **136** and respective upper **138** and lower **140** bone end secured components.

As further depicted in FIG. **14**, an upper reconditioned end-configuration is illustrated at **142** established within the end of the upper femur **2** and exhibits an enlarged spherical surface receiving pocket established between lowermost projection locations of the femur. The upper component **138** is dimensioned to be anchor mounted within the recess profile **142**, the upper component **138** exhibiting a like spherical receiving and flared inner pocket **139** established between a

pair of arcuate edged ears or lobes collectively defining the upper component **138**. As shown in FIG. **13** this in turn eccentrically seats therebetween a majority of the spherical component **136** as shown in FIG. **13**.

As shown in FIG. **14**, the lower tibia leg bone includes an upper bone recess secured pocket **144** (establishing a generally rectangular shaped profile surrounded by a generally flattened lip edge **146**) for receiving the lower bone secured arcuate/concave support **140**. The lower anchoring component **140** exhibits a bottom mounting pedestal or base **148** for seating within the recessed pocket **144** of the tibia bone end face, the component further exhibiting and opposite/upwardly facing and inwardly flared/arcuate track support **150**. In this fashion, the intermediate positioned spherical inter-movable support **136** establishes a limited eccentrically rotatable configuration with the upper leg receiving pocket, combined with a further measure of eccentric support with the lower leg secured arcuate/concave support and again combined with a limited degree of linearly/arcuately translatable motion along the lower leg secured arcuate support pathway;

Referring finally to FIGS. **15** and **16**, respective perspective assembled and exploded illustrations similar to that depicted in FIG. **14** are generally shown at **152** of a modified sub-variant of FIG. **13** and in which an upper femur bone recess configuration **154** exhibits an enlarged/widened inner profile in comparison to that previously shown at **142**, with the lower tibia bone recess configuration again be substantially as depicted at **144** and **146**. The upper anchoring component is depicted as a pair of arcuate/ear shaped an assembleable components **156** and **158** (see further upper end assembling tabs **160** and slots **162** established between the components **156** and **158**).

The ear shaped components **156** and **158** are pre-assembled about a widened and pseudo roller/egg shaped support exhibiting a cylindrically flattened central location **164** with opposite spherical end profiles **166** and **168** (see again as best shown in FIG. **16**), following which the subassembly is installed within the upper recess configuration **142** as depicted in FIG. **15**. A lower anchoring component **170** (similar in respects to that previously described at **140** in FIG. **14**) exhibits a bottom mounting pedestal or base **172** for seating within the recessed pocket **144** of the tibia bone end face, the component further exhibiting and opposite/upwardly facing and inwardly flared/arcuate track support **174**, which is in turn widened in comparison to that previously referenced at **150** for the purpose of supporting the correspondingly widened surface profile of the modified pseudo cylindrical/spherical end shaped intermediate support **164**. The construction **152** therefore provides a further non-limiting example of a more robust joint support assembly of a type contemplated by the present invention.

Having described my invention, other and additional preferred embodiments will become apparent to those skilled in the art to which it pertains, and without deviating from the scope of the appended claims.

We claim:

1. A multi-component joint assembly incorporated into reconditioned end surfaces established between an upper bone and an opposing lower bone, said assembly comprising:
  - a first component adapted to being anchored into the upper reconditioned bone end surface and exhibiting a first exposed support surface;
  - a second component adapted to being anchored into the lower reconditioned bone end surface and exhibiting a second exposed support surface; and
  - a spherical shaped component supported in rotational and linear/arcuate translatable fashion between said first and

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second anchored components, said spherical shaped component further having a multi-layer composition including a softer outer layer and first and second harder interior layers establishing a rotational interface therebetween.

2. The joint assembly as described in claim 1, at least one of said components further exhibiting a hemispherical recess for substantially seating said spherical shaped component.

3. The joint assembly as described in claim 1, each of said first, second and spherical shaped components further being constructed of at least one of a metal, plastic, polymer or composite material.

4. The joint assembly as described in claim 1, further comprising a grid pattern of lubricating grooves defined in a surface of an innermost spherical shaped portion of said spherical component facilitating said rotational interface.

5. A multi-component joint assembly incorporated into reconditioned end surfaces established between an upper bone and an opposing lower bone, said assembly comprising:

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a first component configured to be anchored into the upper reconditioned bone end surface and exhibiting a first exposed support surface having an inwardly flared and elongated profile;

5 a second component configured to be anchored into the lower reconditioned bone end surface and exhibiting a second hemispherical recess shaped support surface; and

a spherical shaped component supported in rotational contact with each of said first and second components, said spherical shaped component also supported in linear/arcuate translatable fashion along said inwardly flared and elongated profile of said first anchored component, said spherical shaped component having a multi-layer composition including a softer outer layer and at least one harder interior layer, said outer and interior layers establishing a rotational interface therebetween.

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